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## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification: <b>A61F 2/01, A61F 2/06</b>	<b>A1</b>	(11) International Publication Number: <b>WO 00/07521</b> (43) International Publication Date: 17 February 2000 (17.02.2000)
(21) International Application Number: <b>PCT/US99/17685</b> (22) International Filing Date: 04 August 1999 (04.08.1999) (30) Priority Data: 09/128,439 04 August 1998 (04.08.1998) US (60) Parent Application or Grant ADVANCED CARDIOVASCULAR SYSTEMS, INC. [/]; () FITZ, Andrew, J. [/]; () MAHER, Pamela, G. ; ()	<b>Published</b>	
(54) Title: <b>ASSEMBLY FOR COLLECTING EMBOLI AND METHOD OF USE</b> (54) Titre: <b>DISPOSITIF DE COLLECTE DE FORMATIONS D'EMBOLES ET PROCEDE D'UTILISATION DUDIT DISPOSITIF</b>  (57) Abstract <p>The present invention is directed to an apparatus and method for treating cerebral blood vessels such as carotid arteries. The system generally includes an apparatus and method for safely and easily deploying a self-expanding stent in a vessel while preventing embolic migration using a filter.</p> (57) Abrégé <p>L'invention concerne un appareil et un procédé de traitement des vaisseaux sanguins cérébraux, tels que les artères carotides. Le système inclut généralement un appareil et un procédé qui permettent de déployer avec sûreté et facilité un stent auto-extensible dans un vaisseau tout en empêchant une migration embolique au moyen d'un filtre.</p>		

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(21) International Application Number: <b>PCT/US99/17685</b> (22) International Filing Date: <b>4 August 1999 (04.08.99)</b> (30) Priority Data: <b>09/128,439 4 August 1998 (04.08.98) US</b> (71) Applicant: <b>ADVANCED CARDIOVASCULAR SYSTEMS, INC. [US/US]; 3200 Lakeside Drive, Santa Clara, CA 95054-8167 (US).</b> (72) Inventor: <b>FITZ, Andrew, J.; 1239 P Henderson Avenue, Sunnyvale, CA 94086 (US).</b> (74) Agents: <b>MAHER, Pamela, G. et al.; Fulwider Patton Lee &amp; Utecht, LLP, 10th floor, 10877 Wilshire Boulevard, Los Angeles, CA 90024 (US).</b>	(81) Designated States: <b>AE, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).</b>  <b>Published</b> <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>	
(54) Title: <b>ASSEMBLY FOR COLLECTING EMBOLI AND METHOD OF USE</b>		
(57) Abstract		
<p>The present invention is directed to an apparatus and method for treating cerebral blood vessels such as carotid arteries. The system generally includes an apparatus and method for safely and easily deploying a self-expanding stent in a vessel while preventing embolic migration using a filter.</p>		

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**Description**

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ASSEMBLY FOR COLLECTING EMBOLI  
AND METHOD OF USE

BACKGROUND OF THE INVENTION

The present invention relates generally to the field of surgical instruments. Specifically, the present invention relates to an emboli-capture device for treating cerebral blood vessels such as carotid arteries.

Stenting and angioplasty in stenosed cerebral vessels (e.g., carotid arteries) pose risks of dislodging thrombus or friable plaque. The thrombus or plaque can become lodged in the brain or arteries and cause serious injury such as a stroke. If such embolic material is dislodged during a stenting procedure, it is necessary to collect the material before it migrates and causes injury. A previous invention, U.S. Patent No. 4,921,478, "Cerebral Balloon Angioplasty System," Solano et al., employs an occlusion catheter carrying a relatively large inflatable occlusion balloon to repair vessels. The balloon is capable of being formed into a funnel while simultaneously sealing a vessel and establishing retrograde blood flow. The balloon is bulky and difficult to refold and withdraw from lesions within the vessels. The withdrawal is prone to causing extensive tissue damage and dislodging more emboli. Moreover, the balloon-type system will not work effectively without a complete and perfect seal between the balloon and the vessel wall. Moreover, Solano et al. contemplates no occlusion in conjunction with the deployment of a self-expanding stent. Further, although the prior art filtered the blood, sometimes excess emboli remained when the device was removed from blood vessels.

What has been needed and heretofore unavailable is a means to deliver and implant a stent in conjunction with a safe and easy-to-use device and method of use for stenting blood vessels while minimizing the risk of embolic migration. The present invention satisfies this need.

SUMMARY OF THE INVENTION

The present invention is directed to an apparatus and method for treating stenosed cerebral blood vessels such as carotid arteries. The system generally includes an apparatus and method for safely and easily deploying a self-expanding stent in a vessel while preventing embolic migration.

In a preferred embodiment, a system for percutaneously delivering a stent within a vessel while preventing embolic migration includes: a restraining sheath that is capable of both expanding and retracting whereby minimal friction is created between the restraining sheath and the stent during deployment of the stent; a filter for trapping and retaining embolic material, the filter being located relative to the restraining sheath such that the filter will trap any embolic material flowing into the restraining sheath; a stent delivery catheter having a proximal end open to atmospheric pressure and a distal end connected to a proximal end of the restraining sheath; and a stent that initially is in a collapsed state and positioned within the restraining sheath.

The filter may consist of one of many devices already in use, e.g., a strainer device comprised of a plurality of wires. The expansion of the restraining sheath may be accomplished by mechanically pushing a composite sheath using a design similar to that of an umbrella.

In another preferred embodiment, expansion of the filter may be accomplished by using a wedge and spine mechanism to open the restraining sheath from a closed position.

In another preferred embodiment, the expansion of the filter may be accomplished by releasing a plurality of bent wires that are restrained in a straightened position.

The sheath design provides optimal deployment of the self-expanding stent because the sheath both expands in a radial direction and retracts in a proximal

5 direction simultaneously. Therefore, due to the angle of incidence created between  
the sheath and the stent during deployment there is a low coefficient of friction  
10 between the sheath and the stent. This is an ideal configuration for recapturing a  
partially deployed stent because contact is constantly maintained between the sheath  
5 and the undeployed part of the stent.

15 A desired site within a vessel is first accessed with the system. The  
restraining sheath then is deployed while being moved proximally. The restraining  
sheath, as it expands, forms an occlusive conical member or catch basin at a  
proximal end of the stent. The stent, being self-expanding, is automatically  
20 deployed as the restraining sheath expands. A temporary seal is created between the  
stent and the restraining sheath. An outer edge of a distal end of the restraining  
sheath may include a material taken from the group of materials consisting of soft  
25 plastic, rubber, and a gel, in order to ensure a proper seal between the sheath and the  
stent. Therefore, unlike the situation where a balloon exerts pressure on a vessel  
15 wall to cause a seal, in the present invention vessel damage is minimized.

30 The filter is located within the restraining sheath at the occlusion site in  
another embodiment.

35 In yet another preferred embodiment, the filter may be located within the  
stent delivery catheter. Alternatively, the filter may be located outside of the  
20 patient's body.

40 Due to the occlusion of the vessel at the proximal end of the stent, a pressure  
differential is created between the more distal arteries (pressurized at blood pressure  
plus atmospheric pressure) and a lumen of the stent delivery catheter (pressurized at  
atmospheric pressure). Therefore, retrograde blood flow is induced and blood and  
45 embolic particles are flushed into the filter where the embolic particles are captured.  
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In another preferred embodiment, a vacuum apparatus may be included in the  
system if the occlusion is not adequate to induce sufficient retrograde blood flow or  
50 to ensure that the maximum number of embolic particles are aspirated into the filter.

5 The restraining sheath is then collapsed to its original size, thereby trapping any remaining embolic material. The system is then removed from the patient.

10 Other features and advantages of the present invention will become more apparent from the following detailed description of the invention when taken in  
5 conjunction with the accompanying exemplary drawings.

15 BRIEF DESCRIPTION OF THE DRAWINGS

20 FIGURE 1 is a perspective view of one embodiment, depicting in a closed position an apparatus of a composite design similar to that of an umbrella for expanding a restraining sheath wherein expansion is accomplished by mechanically  
10 pushing the sheath.

25 FIG. 2 is a perspective view of the apparatus of FIG. 1 depicted in an open position.

30 FIG. 3 is a perspective view of another embodiment depicting an apparatus in a closed position for expanding the restraining sheath wherein expansion is  
35 15 accomplished by using a wedge and spine mechanism to open the restraining sheath from a closed position.

40 FIG. 4 is a perspective view of the apparatus of FIG. 3 in a partially expanded position.

45 20 FIG. 5 is a perspective view of the apparatus of FIG. 3 in a fully expanded position.



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FIG. 6 is a perspective view of another preferred embodiment depicting an apparatus in a closed position for expanding the restraining sheath wherein expansion is accomplished by releasing bent wires that are restrained in a straightened position.

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FIG. 7 is a perspective view of the apparatus of FIG. 6 in a fully expanded position.

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FIG. 8 is a cross-sectional view of a restraining sheath in a closed position.

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FIG. 9 is a perspective view of a restraining sheath that has been partially expanded by the apparatus of FIG. 3.

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FIG. 10 is a perspective view of a restraining sheath that has been partially expanded by the apparatus of FIG. 6.

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FIG. 11 is an elevational view of the present invention, partially in cross-section, after advancement to a desired vessel site and just prior to commencement of stent deployment.

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FIG. 12 is an elevational view, partially in cross-section, depicting the present invention during stent deployment.

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FIG. 13 is an elevational view, partially in cross-section, depicting the present invention after the stent has been fully deployed.

FIG. 14 is an elevational view, partially in cross-section, depicting the present invention after the stent has been fully deployed, including an optional vacuum apparatus.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

As shown in the exemplary drawings, the present invention may be embodied in various ways. Where common elements occur in more than one embodiment, the same reference numerals will be used. Referring to FIG. 1, depicting one preferred embodiment, an apparatus 10 of a composite design similar to that of an umbrella for expanding a restraining sheath is shown. The restraining sheath is omitted for clarity. A stent delivery catheter 12 is coaxially positioned within the apparatus 10. Expansion of the restraining sheath is accomplished by mechanically pushing the sheath via expansion of an expandable cage 14. The cage 14 consists of spines 16 each of which have bends 18. The spines 16 are secured by a fixed support ring 20 at the proximal end of spines 16. A distal end of a control wire 22 is fixed to a collar 24 that is slidably mounted about the delivery catheter. The cage is expanded by pulling the collar proximally via the control wire which causes secondary spines 26 (see FIG. 2) to press against the larger spines 16. One end of each secondary spine 26 is pivotally secured to the collar 24. The opposing end of each secondary spine is pivotally secured to larger spine 26. Likewise, the proximal end of each larger spine 16 is pivotally secured to the fixed control ring 20. As a result, the cage 14 pushes outwardly on the sheath membrane and the sheath thus expands at a distal end and forms a catch basin.

In another preferred embodiment, an apparatus 30 provides expansion for the sheath membrane (omitted for clarity), as shown in FIG. 3. A plurality of spines 32 project distally and function to support the sheath. The spines 32 are pivotally secured at their proximal ends to the stent delivery catheter 12. A wedge 34 is

-7-

5 slidably mounted on the stent delivery catheter and may be moved axially relative to the catheter and the spines 32 by a control wire (omitted for clarity) or other means.

10 As shown in FIG. 4, when the wedge 34 is moved proximally relative to the spines, the wedge forces the spines to protrude outwardly in a radial direction.

5 FIG. 5 depicts the spines in a fully expanded position. The wedge has been moved as far as possible in a proximal direction.

15 As shown in FIG. 6, an apparatus 40 for expanding the sheath membrane (omitted for clarity) provides yet another preferred embodiment. A plurality of bent wires 42 are restrained in a straightened position by a fixed restraint ring 44 at a  
20 proximal end of the apparatus 40 and slidably mounted restraint ring 46 at a distal end of the apparatus. The slidably mounted restraint ring is initially positioned at the distal ends of the wires 42. A catheter 12 is coaxially positioned within the  
25 wires 42 and the rings 44,46. A second control wire 48 is attached to the slidably mounted restraint ring.

15 Referring to FIG. 7, the slidably mounted restraint ring 46 has been moved proximally via the second control wire. The wires 42 have thus been released and  
30 have sprung into their resting bent positions. This action serves to fully expand a restraining sheath.

35 Turning to FIG. 8, a restraining sheath 50 is depicted and is supported by  
20 spines 52, or alternatively wires. The restraining sheath in a closed position may consist of folds 54. An alternative to providing folds 54 is to construct a restraining  
40 sheath of a material that is capable of being stretched in a radial direction. This alternative would require less material but would require more force to expand the material in a radial direction than would be required if folds were implemented. A  
45 restraining sheath may be formed from a material selected from the group of materials consisting of polyethylene, polyester, and polyamide. The material, which  
50 has a low coefficient of friction, may be obtained in varying grades of softness.

5 As shown in FIG. 9, the restraining sheath 56 may be expanded by the apparatus 30 of FIG. 3 such that the diameter at the distal end is larger than the diameter at the proximal end.

10 Turning to FIG. 10, the restraining sheath 58 may be expanded by the apparatus of FIG. 6 such that the diameter at the distal end is larger than the diameter at the proximal end.

15 The sheath design provides optimal deployment of the self-expanding stent because the sheath both expands in a radial direction and retracts in a proximal direction simultaneously. Therefore, due to the angle of incidence created between the sheath and the stent during deployment, there is a low coefficient of friction between the sheath and the stent. This is an ideal configuration for recapturing a partially deployed stent because contact is constantly maintained between the sheath and the undeployed part of the stent.

20 Turning to FIGS. 11-13, in a preferred method, a desired site within vessel 60 is first accessed with the system, via a percutaneous technique. A stent delivery catheter 62 has its proximal end open to atmospheric pressure and its distal end running into the proximal end of restraining sheath 64. A self-expanding stent 66 is initially in a collapsed state and partially disposed within the restraining sheath. The restraining sheath then is deployed, and as it expands, the restraining sheath forms an occlusive conical member 68 or a catch basin at the proximal end of the stent. The stent, being of the self-expanding type, is automatically deployed as the restraining sheath expands. A temporary seal is created between the stent and the restraining sheath. The outer edge of the distal end of restraining sheath 64 may include a material consisting of soft plastic, rubber, or a gel, in order to ensure a proper seal between the sheath and the stent. Therefore, unlike the situation where a balloon exerts pressure on a vessel wall to cause a seal, in the present invention vessel damage is minimized.

5 A filter 70 for trapping and retaining embolic material or particles 72 is  
located relative to the restraining sheath 64 such that the filter will trap any embolic  
10 material flowing into the restraining sheath. Such filters are known in the art and  
may include a strainer device comprised of a plurality of wires. The filter may be  
5 located within the restraining sheath at the occlusion site one embodiment. In  
another embodiment, the filter 70 may be located within the stent delivery catheter  
15 62, as shown in phantom in FIG. 13. In yet another preferred embodiment, the filter  
may be located outside of the patient's body (not shown).

20 Due to the occlusion of the vessel 60 at the proximal end of the stent 66, a  
10 pressure differential is created between the more distal arteries (pressurized at blood  
pressure plus atmospheric pressure) and a lumen of the stent delivery catheter  
(pressurized at atmospheric pressure). Therefore, retrograde blood flow is induced  
25 and blood and embolic particles are flushed into the filter 70 where the embolic  
particles are collected.

15 Turning to FIG. 14, in another preferred embodiment an aspiration system  
30 consisting of a vacuum device 74 with an optional valve 76 may be included in the  
system if the occlusion is not adequate to induce sufficient retrograde blood flow or  
to ensure that the maximum number of embolic particles 72 is aspirated into the  
35 filter 70. Alternatively, in another embodiment, an aspiration system consisting of a  
20 luer lock (not shown) capable of accepting a syringe may be used.

40 The restraining sheath 64 then is collapsed to its original size, thereby  
trapping any remaining embolic material or particles 72. The system is then  
removed from the patient. Thus, a self-expanding stent is deployed safely and  
easily without the risk of embolic migration.

45 25 While the invention has been illustrated and described herein in terms of its  
use as a safe and easy-to-use apparatus and method for treating blood vessels while  
minimizing the risk of embolic migration, it will be apparent to those skilled in the  
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art that the invention can be used in other instances. Other modifications and improvements may be made without departing from the scope of the invention.

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## Claims

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WHAT IS CLAIMED IS:

1. A system for delivering a stent within a vessel while preventing embolization, comprising:  
a restraining sheath adapted for expanding and retracting whereby minimal friction exists between the restraining sheath and the stent during deployment of the stent;  
a filter for collecting and retaining embolic material, the filter being located relative to the restraining sheath so that the filter collects any embolic material flowing into the restraining sheath; and  
a stent delivery catheter having a proximal end open to atmospheric pressure and a distal end running into a proximal end of the restraining sheath; whereby the stent initially is in a low-profile, collapsed state and positioned within the restraining sheath.

2. The system of claim 1, wherein the restraining sheath is formed from a material that has a low coefficient of friction.

3. The system of claim 1, wherein the restraining sheath is formed from a material selected from the group of materials consisting of polyethylene, polyester, polyamide, peba, silicone, rubber, nylon and elastomers.

4. The system of claim 1, wherein the restraining sheath is formed from a material that may be obtained in varying grades of softness.



5                   5. The system of claim 2, wherein the restraining sheath expands to form a catch basin.

10                   6. The system of claim 2, wherein an outer edge of a distal end of the restraining sheath includes a material taken from the group of materials consisting of soft plastic, rubber, and a gel, thereby ensuring a seal between the sheath and the  
15                   stent.

20                   7. The system of claim 2, wherein the restraining sheath includes a plurality of folds for expanding from a closed position to an open position.

25                   8. The system of claim 2, wherein the restraining sheath is formed from an elastic material so that the restraining sheath can be stretched from a closed to an open position.

30                   9. The system of claim 2, wherein expansion of the restraining sheath may be accomplished by an apparatus including an expandable cage having a plurality of first spines, each of the first spines including a bend and being pivotally secured by  
35                   a fixed support ring at a proximal end, the apparatus further including a plurality of secondary spines, each of the secondary spines being pivotally secured at a proximal  
40                   end to one of each of the first spines and being pivotally secured at a distal end to a slidably mounted collar, the cage pushing outwardly on the sheath when the collar is moved proximally.

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5                   10. The system of claim 2, wherein a wedge and a spine mechanism move  
the restraining sheath from a closed position to an open position.

10                   11. The system of claim 2, wherein one or more restrained spring elements  
are provided to expand the restraining sheath.

15                   12. The system of claim 11, wherein a plurality of bent wires being  
associated with the restraining sheath, the bent wires being restrained in a  
straightened position and when released expand the restraining sheath.

20                   13. The system of claim 12, further including a restraint ring for retaining  
the bent wires in a straightened position.

25                   14. The system of claim 13, further including a fixed support ring for  
supporting the bent wires at a proximal end.

30                   15. The system of claim 1, wherein the filter is located within the restraining  
sheath.

35                   16. The system of claim 1, wherein the filter is located within the stent  
delivery catheter.

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5 17. The system of claim 1, wherein the filter is located outside of the body of  
a patient.

10 18. The system of claim 1, further including an aspiration system for  
aspirating embolic material into the stent delivery catheter.

15 19. The system of claim 18, wherein the aspiration system attaches the stent  
20 delivery catheter by a luer lock fitting.

25 20. The system of claim 19, wherein the luer lock is capable of accepting a  
syringe for facilitating the aspiration of embolic material into the stent delivery  
30 catheter.

35 21. The system of claim 18, wherein the aspiration system includes a  
vacuum apparatus for inducing retrograde blood flow.

40 22. The system of claim 21, wherein the vacuum apparatus includes a valve  
for facilitating rapid activation of the vacuum apparatus.

45 23. The system of claim 1, wherein the stent is self-expanding.

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24. A method for deploying a self-expanding stent within a vessel while simultaneously preventing the migration of embolic material, using a system including a restraining sheath, a filter, a stent delivery catheter having a proximal end open to atmospheric pressure and a distal end running into a proximal end of the restraining sheath, and a self-expanding stent, comprising the steps of:  
accessing a desired site within the vessel with the system;  
deploying the restraining sheath while moving the sheath proximally, thereby forming a catch basin and simultaneously deploying and implanting the self-expanding stent, the catch basin occluding the vessel at a proximal end of the stent, thereby inducing retrograde blood flow through the filter;  
collapsing the restraining sheath and collecting any remaining embolic material; and  
removing the system from the patient.

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25. A method for deploying a self-expanding stent within a vessel while simultaneously capturing a resultant emboli, using a system including a restraining sheath, a filter, a stent delivery catheter having a proximal end open to atmospheric pressure and a distal end running into a proximal end of the restraining sheath, a vacuum apparatus, and a self-expanding stent, comprising the steps of:  
accessing a desired site within the vessel with the system;  
deploying the restraining sheath while moving the sheath proximally, thus causing the formation of a catch basin and the automatic deployment of the stent, the catch basin occluding the vessel at a proximal end of the stent, thereby inducing retrograde blood flow through the filter;  
activating the vacuum apparatus to maximize the aspiration of embolic material into the filter;

5 collapsing the restraining sheath to its original size, thus collecting  
any remaining embolic material; and  
10 15 removing the system from the patient.

15 26. A method of creating a pressure differential in a vessel to collect embolic  
material by creating a substantially atraumatic seal across a lesion within the vessel  
while preventing embolization.

20 27. The method of claim 26, further including activating a vacuum apparatus  
to maximize the amount of embolic material that is aspirated into a filter.  
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I/II

FIG. 1

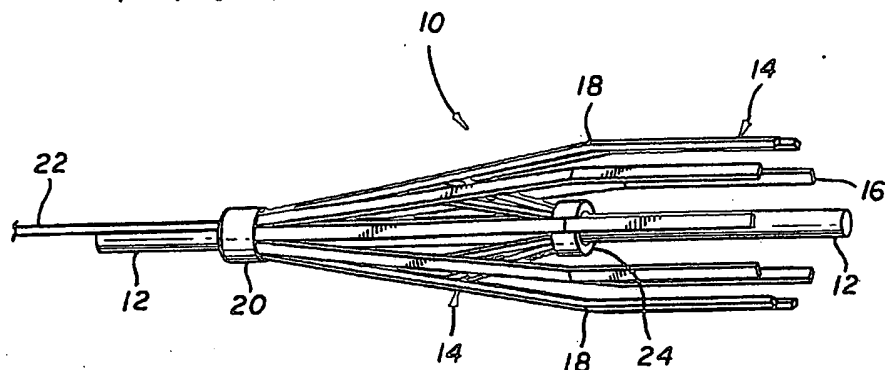
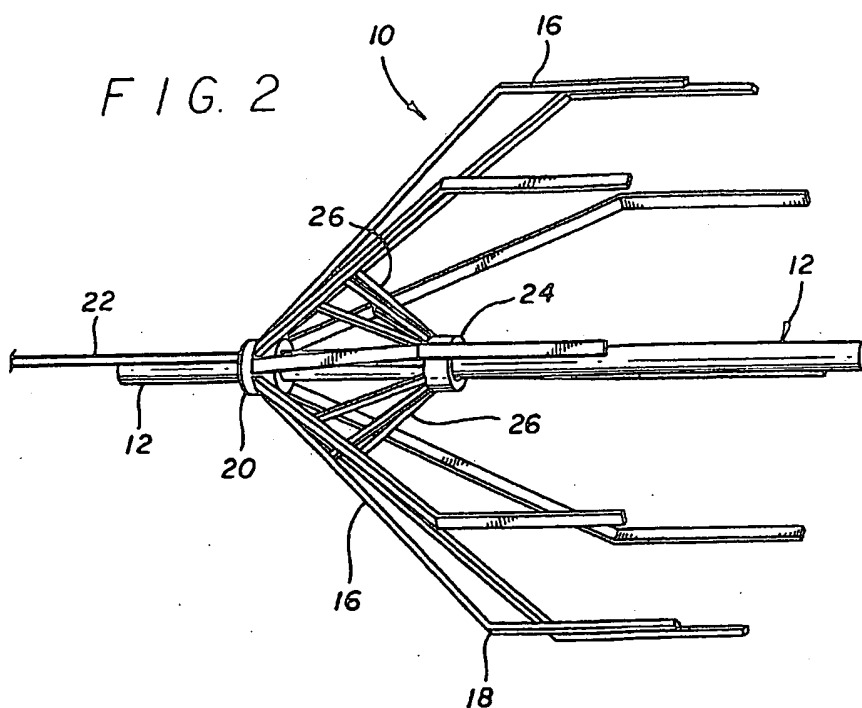


FIG. 2



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FIG. 3

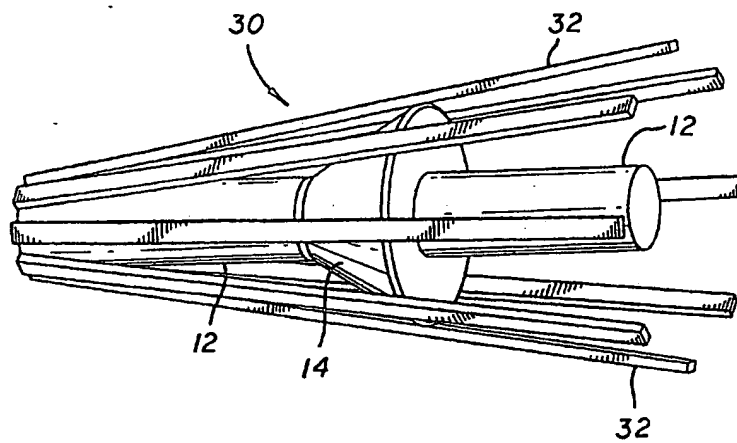
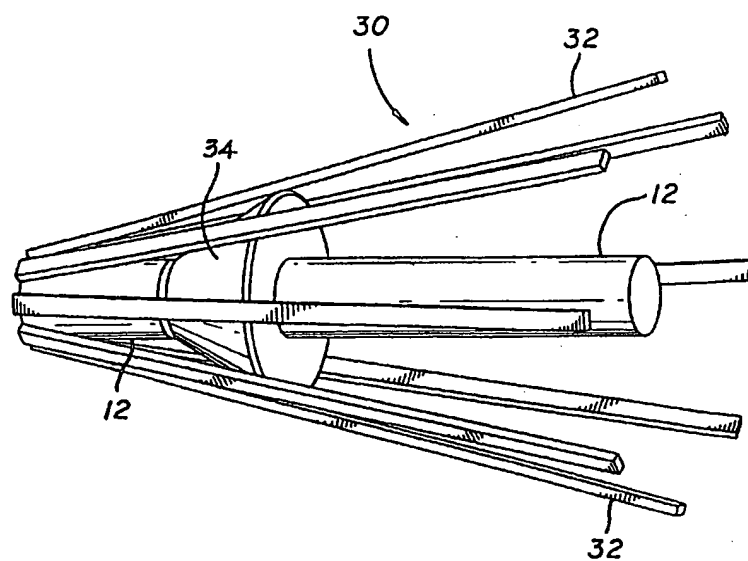
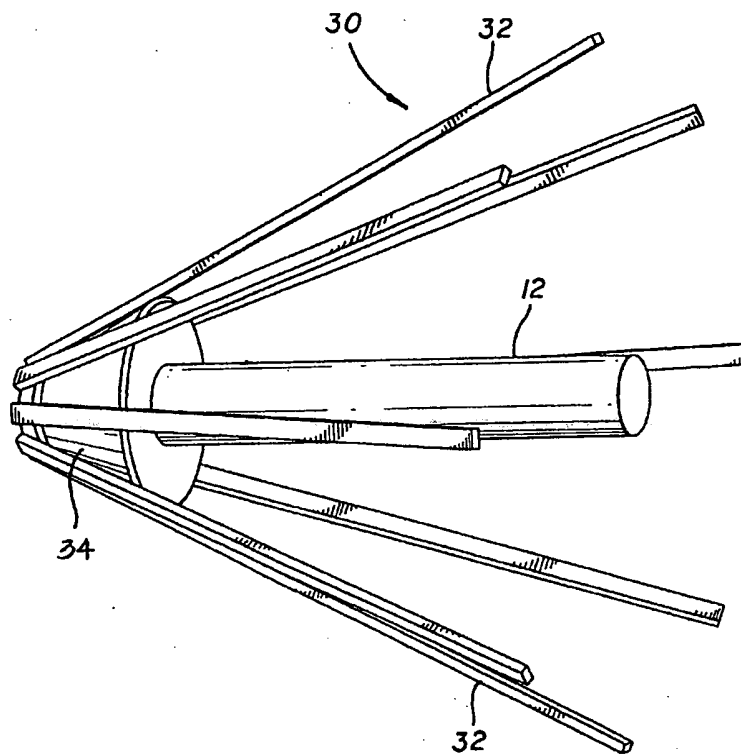


FIG. 4



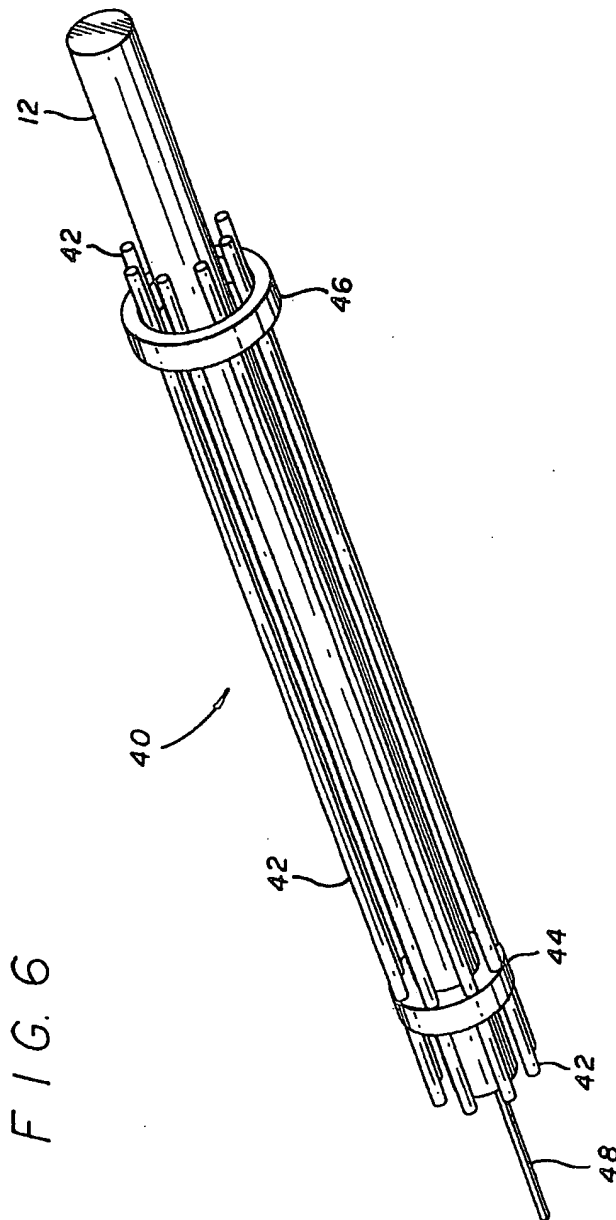
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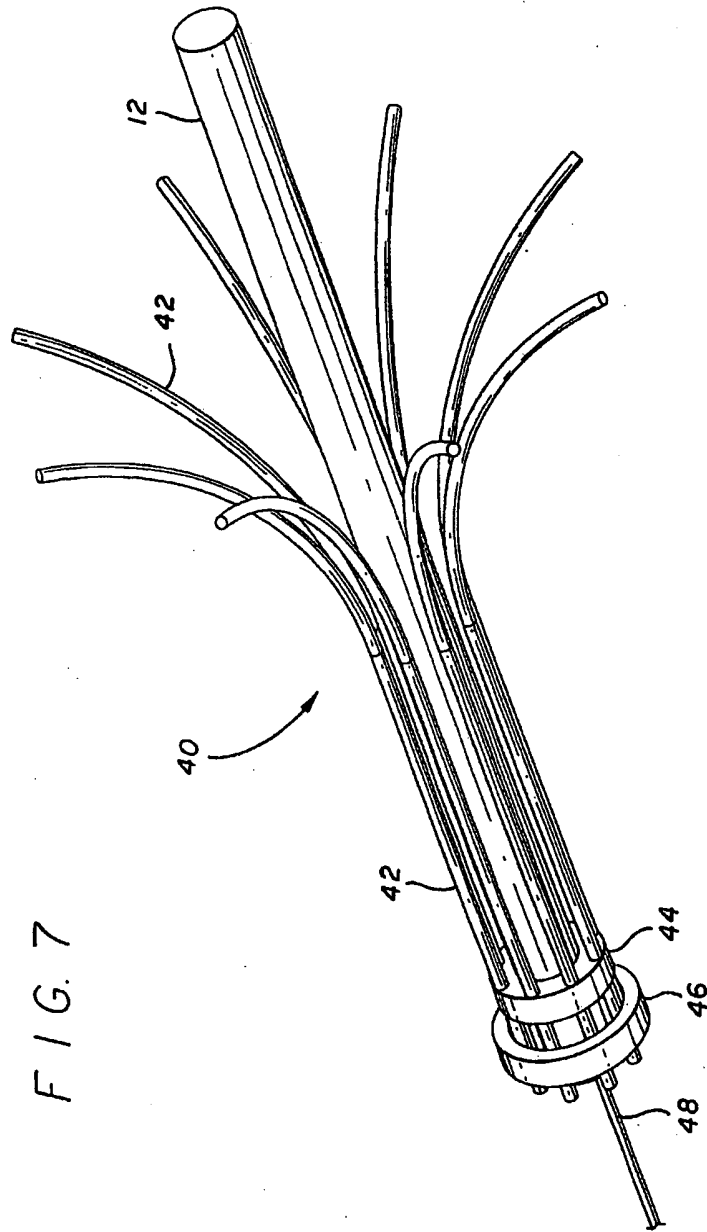
FIG. 5





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6/11

FIG. 8

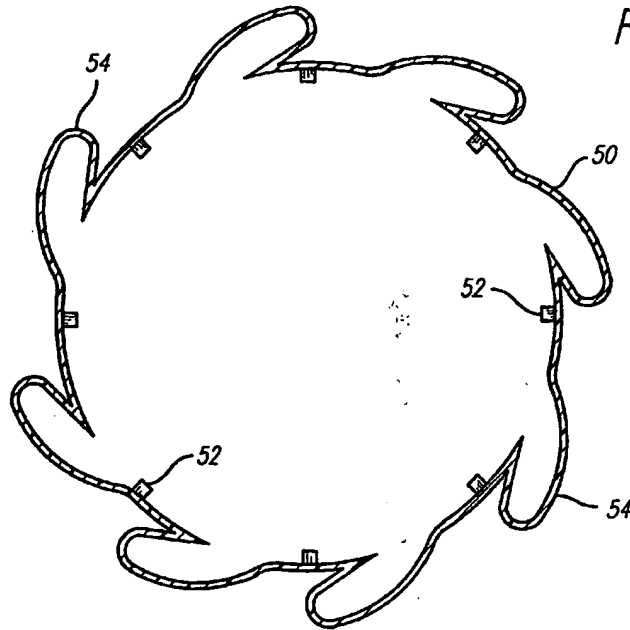


FIG. 9

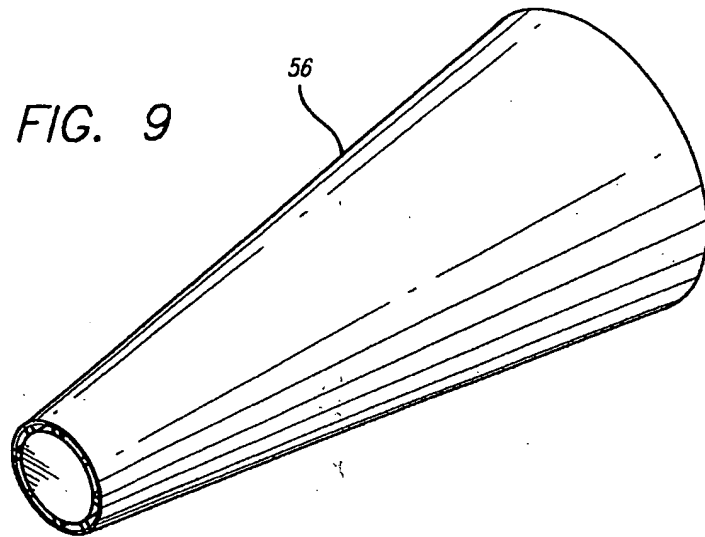


FIG. 10

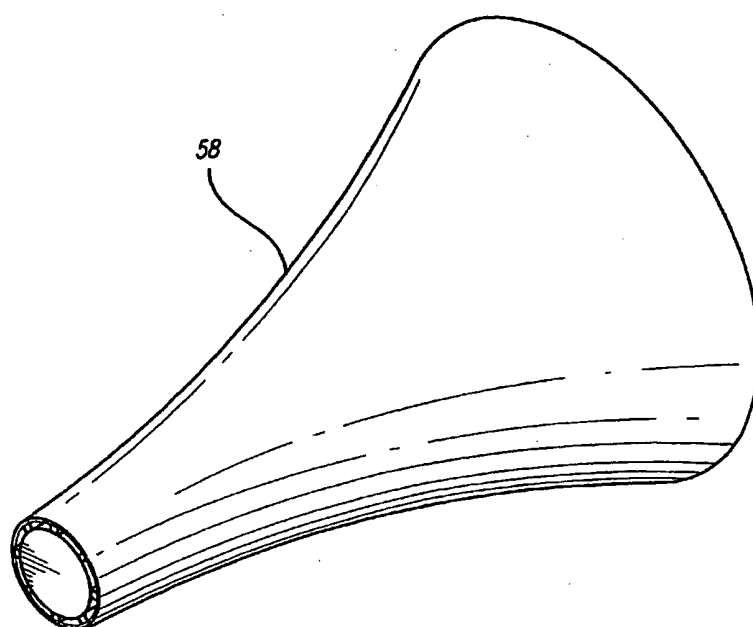
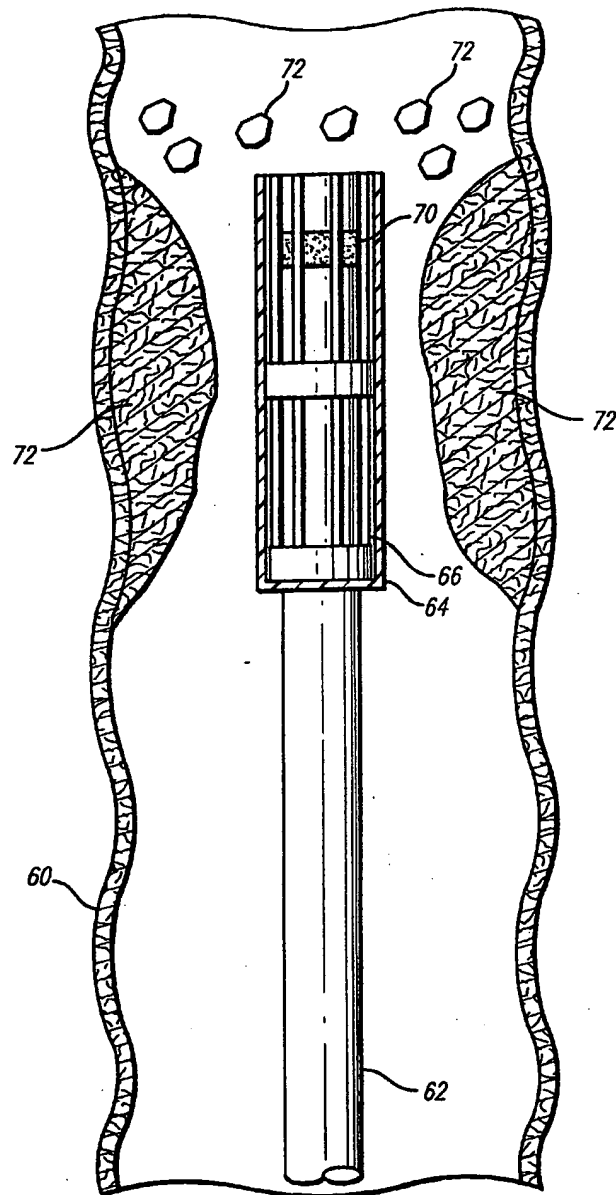


FIG. 11



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FIG. 12

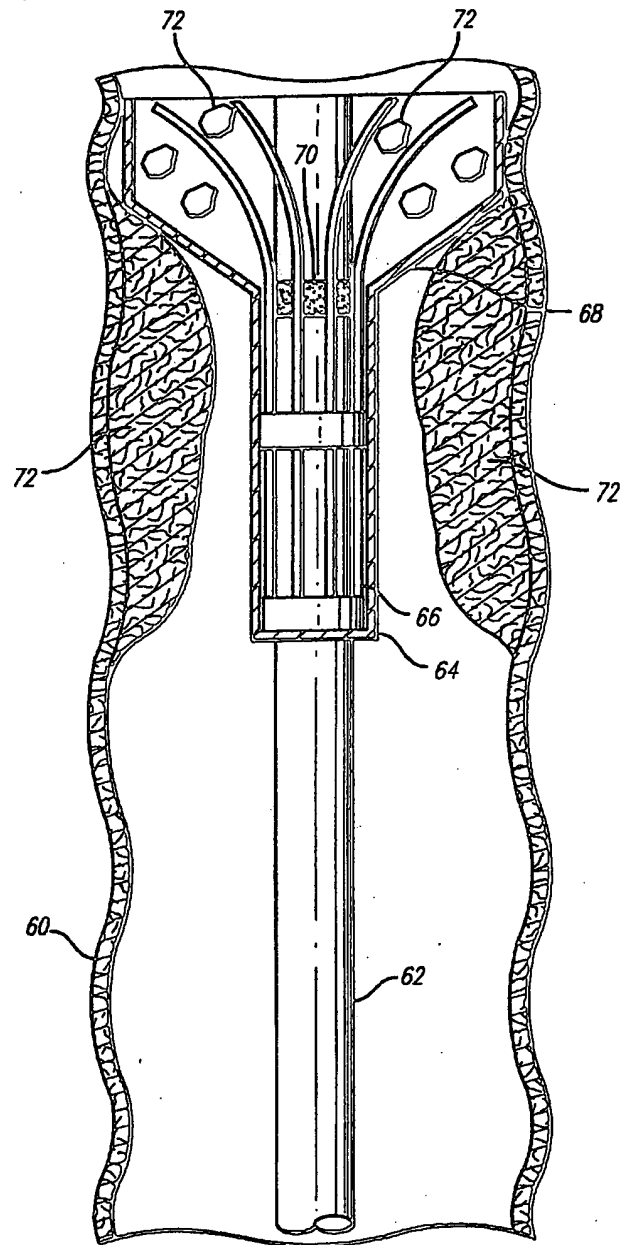


FIG. 13

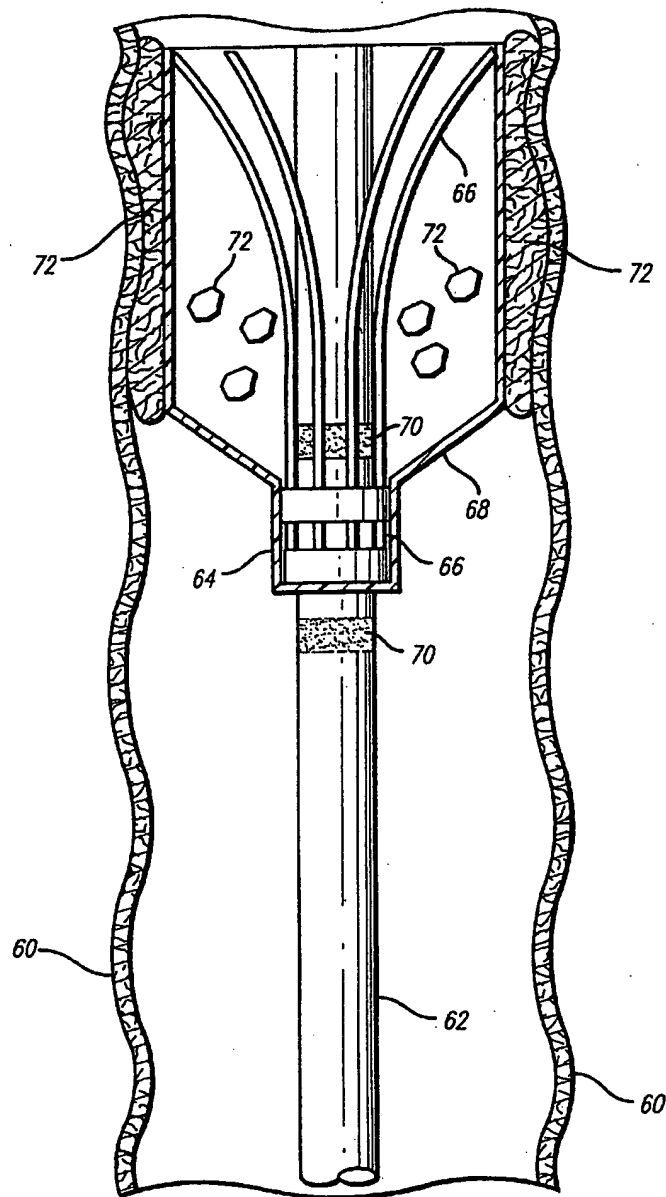
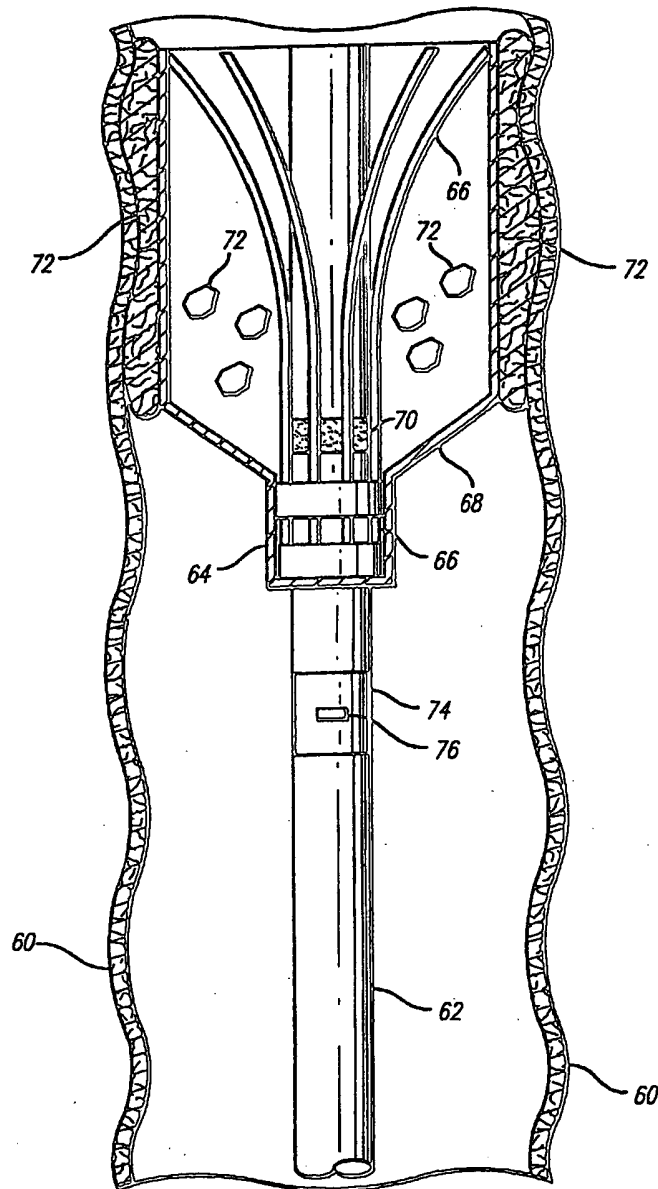


FIG. 14





# INTERNATIONAL SEARCH REPORT

Int. Patent Application No.  
PCT/US 99/17685

A. CLASSIFICATION OF SUBJECT MATTER  
IPC 7 A61F2/01 A61F2/06

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)  
IPC 7 A61F A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 713 917 A (TAHERI SYDE A ET AL) 3 February 1998 (1998-02-03) figure 8 column 8, line 8 - line 33 column 9, line 6 - line 12 column 10, line 66 - column 11, line 41 column 13, line 9 - line 27 claims 1,14,26	1-3,6,8, 11,12,23
A		4,7,15, 16
X	EP 0 701 800 A (BARD INC C R) 20 March 1996 (1996-03-20) column 7, line 51 - column 8, line 29 column 12, line 52 - column 14, line 10 figures 1,13,15-17,19-23 -/-	1,10

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

### \* Special categories of cited documents:

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Date of the actual completion of the international search

10 December 1999

Date of mailing of the international search report

17/12/1999

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Authorized officer

Mary, C

# INTERNATIONAL SEARCH REPORT

Int. Patent Application No.  
PCT/US 99/17685

C. (Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of documents, with indication where appropriate, of the relevant passages	Relevant to claim No.
P, X	US 5 800 525 A (GOLDSTEEN DAVID S ET AL) 1 September 1998 (1998-09-01)  figures 1,3,7 column 2, line 38 -column 4, line 12 column 4, line 50 - line 60 column 5, line 45 -column 6, line 16	1-3,5,8, 9,11-13, 15,16,23
A		4,7,14
P, X	US 5 882 329 A (HILLIAMS G RONALD ET AL) 16 March 1999 (1999-03-16) figures 18,19 column 8, line 14 -column 10, line 10 column 11, line 25 - line 64 column 13, line 57 -column 14, line 54 column 15, line 14 -column 17, line 40	1
P, A	US 5 800 457 A (GELBFISH GARY A) 1 September 1998 (1998-09-01) figures 1-3 column 6, line 46 -column 7, line 50 column 10, line 7 -column 12, line 31	1,17-22

Form PCT/ISA210 (second sheet) (July 1993)

# INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 99/17685

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: 24-27  
because they relate to subject matter not required to be searched by this Authority, namely:  
Rule 39.1(iv) PCT- Method for treatment of the human or animal body by surgery
2. ☐ Claims Nos.:  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this International application, as follows:

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2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

# INTERNATIONAL SEARCH REPORT

Information on patent family members

In Patent Application No  
PCT/US 99/17685

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US 5800457 A	01-09-1998	NONE	

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